

1 Proof of Concept of the Electrochemical Sensing of 3-iodothyronamine
2 (T₁AM) and Thyronamine (T₀AM)

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25 **Abstract (925/1000 characters)**

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28 It is shown in recent studies that besides the well-recognized T_3 and T_4 there are other relevant
29 thyroid hormones circulating in the human body. In particular this is the case for 3-
30 iodothyronamine (T_1AM) and thyronamine (T_0AM). One of the reasons for the lack of studies
31 showing its precise importance is the absence of analytical methodologies available. Herein, for
32 the first time, T_1AM and T_0AM are electrochemically characterized. T_0AM was sensed by means
33 of a glassy carbon electrode; interestingly T_1AM was sensed both with a graphitic surface
34 (oxidatively) as well as with mercury (reductively). With both compounds it was possible to,
35 subsequently to oxidation, to observe the reversible redox reaction concerning the couple
36 benzoquinone/hydroquinone, thus increasing the specificity of the electroanalysis. *Ergo*, this
37 work provides the basis for an 'at-point-of-use' electrochemical strips test for T_1AM and T_0AM .

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40 **Keywords (max. 5)**

41 Clinical analysis

42 Cyclic voltammetry

43 Electrochemistry

44 Hormones

45 Thyroid

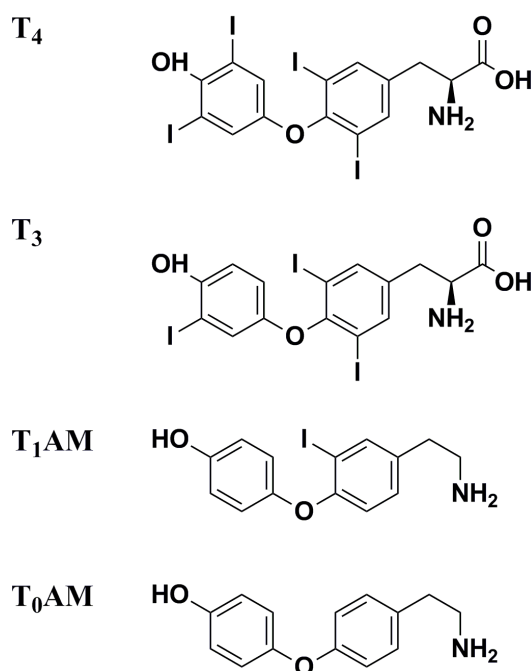
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47 The biological relevance of a hormone stems from its definition: it is a chemical
48 messenger that transports a signal from one cell to another. The thyroid, anatomically situated
49 in the neck produces several hormones, particularly 3',5',3,5-L-tetraiodothyronine (T₄) and
50 3',5',3-L-triiodothyronine (T₃) (Figure 1). Given their importance in several physiological
51 functions, these thyroid hormones are routinely quantified to help diagnose and assess several
52 pathologies.^[1]

53 Thyroid hormones have crucial effects on metabolism and thermogenesis, on processes
54 involving muscular contraction, growth, reproduction, immune and antiviral defense as well as
55 defense against free radicals.^[1] These functions are not specific to the human species, since
56 exactly the same molecules produce similar effects in most vertebrates.^[1] In human plasma,
57 unbound T₄ and T₃ are in the picomolar range, while T₄ and T₃ bound to thyroid-binding-proteins
58 (mainly thyroxine-binding globulin, transthyretin and albumin) is regulated in the nanomolar
59 range.^[1]

60 Less than ten years ago a previously unsuspected thyroid hormone, T₁AM (3-
61 iodothyronamine), was unveiled as a new biologically active thyroid hormone derivative (Figure
62 1).^[2] Later, experiments in small mammals showed that systemic T₁AM and T₀AM (thyronamine)
63 produced hypothermia, a cardiac reversible dose-dependent negative inotropic effect^[3] and a
64 rapid increase in blood glucose.^[4] These data support the notion that these two hormones, like
65 T₃ and T₄, play a role in the regulation of metabolism.

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Figure 1 – Molecular structures of T₄, T₃, T₁AM and T₀AM.

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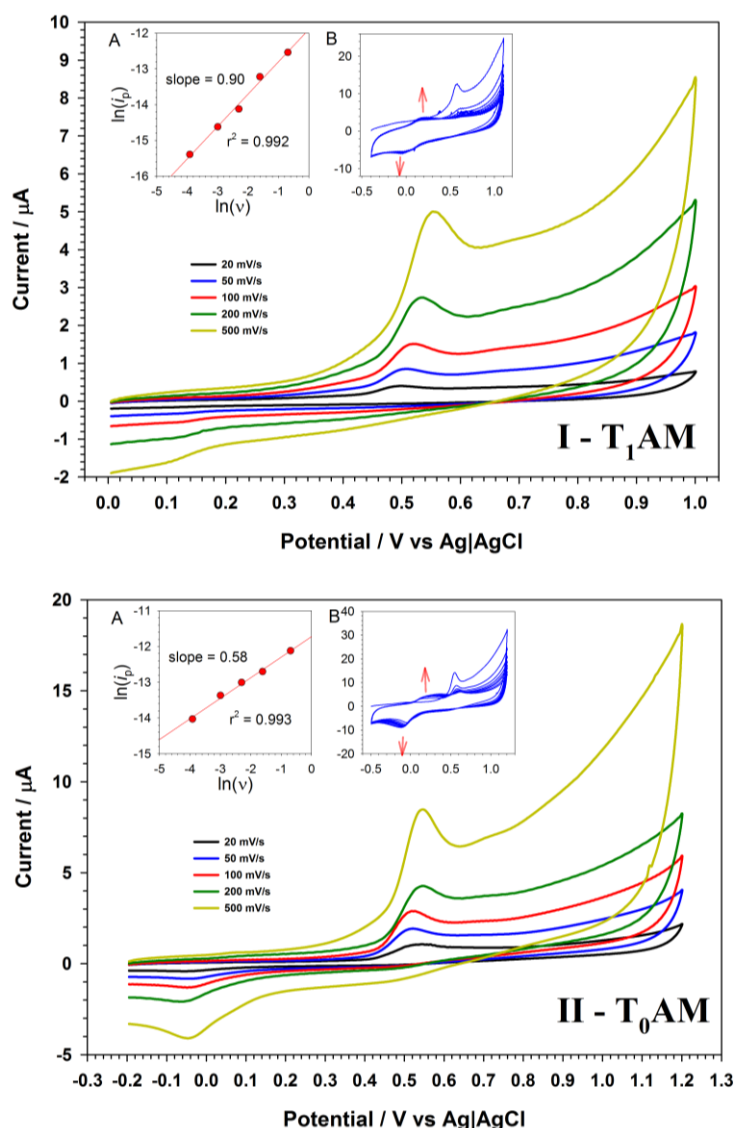
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This leads to compelling, as yet unanswered, questions such as: how much T₁AM and T₀AM circulate in the human body?; how are they distributed?; which metabolic programs are influenced by them?; in which concentrations are they physiological or pathological?; can they be used to treat any pathological process?; can they help in difficult endocrinological differential diagnosis?

76 Answering these questions requires a simple and reliable way to quantify T₁AM and
 77 T₀AM.^[5] So far, their detection and quantification has been based on liquid chromatography with
 78 tandem mass spectrometry detection (LC-MS/MS)^[6] and immunoassay methodologies^[7], which
 79 are laborious and costly. This manuscript advocates the case that electroanalysis may be a viable
 80 and low-cost alternative.

81 Although T₄ and T₃ have been electroanalyzed,^[8] to the best of our knowledge, neither
 82 T₁AM nor T₀AM were ever electrochemically studied before this work. Herein, T₁AM and T₀AM
 83 are successfully analyzed with a glassy carbon electrode (GCE) (Figure 2), in an oxidative
 84 electrode reaction, and also T₁AM with hanging mercury drop electrode (HMDE) (Figure 3), in a
 85 reductive electrode reaction.

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89 *Figure 2 – I – Cyclic voltammograms of aqueous phosphate buffer solution (pH 7) containing 0.174 mM*
 90 *of T₁AM on a GCE, cyclic voltammetry was run between 0.0 and +1.0 V vs. Ag|AgCl at different scan*
 91 *rates. Inlay A: logarithm of scan rate vs. logarithm of peak current. Inlay B: Sequential cyclic*
 92 *voltammograms at 1000 mV/s showing the appearance of a reductive and an oxidative peak around 0.0*
 93 *and +0.2 V vs. Ag|AgCl, respectively. II – Cyclic voltammograms of aqueous phosphate buffer solution*

(pH 7) containing 0.153 mM of T_0AM on a GCE, cyclic voltammetry was run between -0.2 and +1.2 V vs. Ag|AgCl at different scan rates. Inlay A: logarithm of scan rate vs. logarithm of peak current. Inlay B: Sequential cyclic voltammograms at 1000 mV/s showing the appearance of a reductive and an oxidative peak around +0.0 and +0.2 V vs. Ag|AgCl, respectively.

The oxidative processes in a GCE electrode, at pH 7, gives origin to voltammetric signals with peak potential of ca. +0.5 V vs Ag|AgCl.

Considering that a fully irreversible diffusion-only system follows the Randles–Ševčík equation:^[9]

$$i_p = 0.496\sqrt{\alpha + n'}FnAC^* \sqrt{\frac{FDv}{RT}} \quad (1)$$

where i_p is peak current, v is the scan rate, n' is the number of electrons transferred before the rate determining step, n is the total number of electrons transferred, A is the area of the electrode surface, α is the Tafel coefficient (or transfer coefficient), D is the diffusion coefficient of the species, C^* is the bulk concentration of the species, F is the Faraday constant, R is the ideal gas constant, T is the temperature.^[10] Note that equation utilizes the *multi-electron* form of the Randles–Ševčík equation^[11] and is consistent with recent IUPAC recommendations on the definition of the transfer coefficient.^[10]

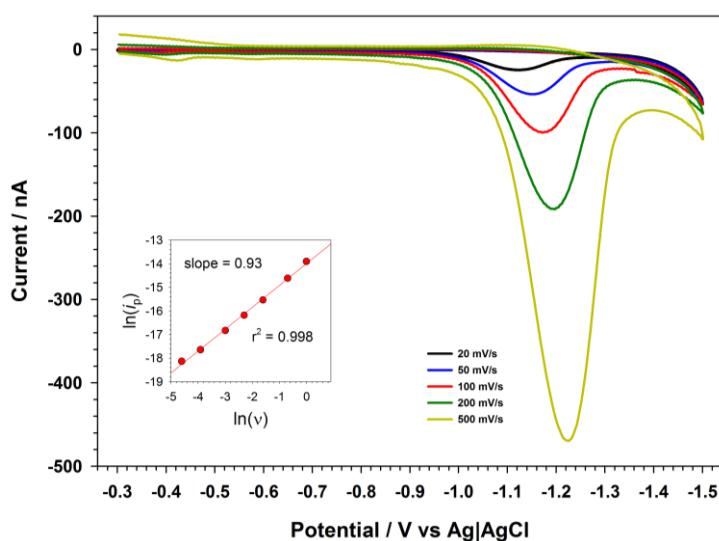


Figure 3 – Cyclic voltammograms of aqueous phosphate buffer solution (pH 7) containing 0.174 mM of T_1AM on a HMDE, cyclic voltammetry was run between -0.3 and -1.5 V vs. Ag|AgCl at different scan rates. Inlay: logarithm of scan rate vs. logarithm of peak current.

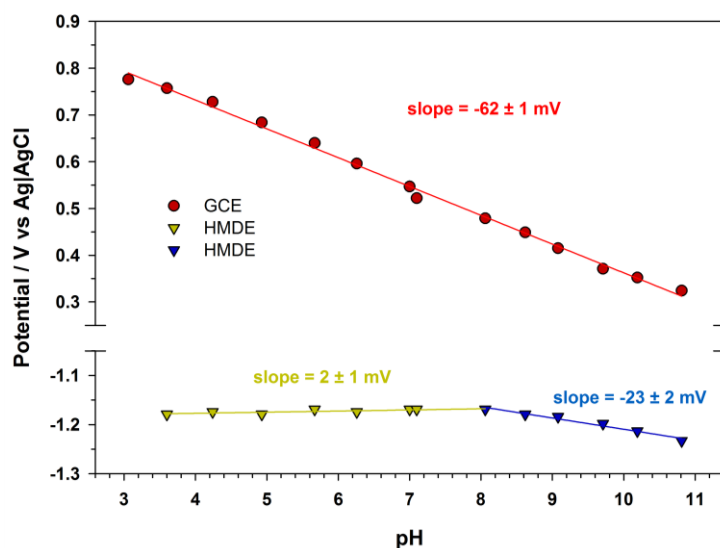
For an irreversible surface bound species, i_p vs. v is given by the following equation:^[11]

$$i_p = \frac{(\alpha + n')nF^2}{2.718RT} vA\Gamma \quad (2)$$

124 where Γ is the surface coverage. Surface and diffusional controlled voltammetric
 125 processes can be distinguished on their scan rate dependence. A direct dependence on the
 126 voltage scan rate, v , corresponds to the former, whereas a square root dependence signals the
 127 latter.^[12] This means that a logarithm of peak current ($\ln|i_p|$) vs. logarithm of scan rate ($\ln|v|$)
 128 will give rise to a slope close to 0.5 in case of a fully diffusional process and a slope close to 1.0
 129 for a fully adsorptive process, both apply to either a spherical or a plane macro-electrode. As
 130 can be seen in the inlay A of Figure 2 - I, a slope ca. 0.9 ± 0.1 suggests an adsorptive process,
 131 which could be expected considering T_1AM molecular structure, a π - π overlapping could occur
 132 between T_1AM and the graphitic surface. However, considering that for T_0AM (inlay A of Figure
 133 2 - II) a slope closer to 0.5 leads the authors to speculate it is the highly polarizable iodine atoms
 134 that indeed promote adsorption. Plots showing the dependence of the peak current on scan
 135 rate and the square root of scan rate are shown in the Supporting Information.

136 For the oxidative reaction (i.e. using the GCE) considering a peak potential vs. pH slope
 137 of 62 mV (Figure 4), i.e. ca. 59 mV,^[11] the electrochemical reaction up to the rate determining
 138 step should have involved an equal number of protons and electrons. It is herein suggested that,
 139 first there is the electrochemically reversible withdraw of 1 electron 1 proton, then, second a
 140 chemically irreversible step where another electron and another proton are removed along with
 141 addition of a water molecule. This cleavages the ether linkage forming *p*-benzoquinone and an
 142 hydroxyl group is introduced in an *ortho* position to the iodine atom (reaction A of Figure 5). By
 143 means of using a fast scan rate, immediately after the oxidative electrochemical reaction one
 144 can observe the benzoquinone/hydroquinone reversible redox reaction at potential around 0.1
 145 V vs. Ag|AgCl (inlay B of Figure 2). A cyclic voltammogram of benzoquinone in the media using
 146 the same voltammetric conditions gave origin to a similar peak with similar peak potential thus
 147 confirming such assumption (data shown in the Supporting Information).

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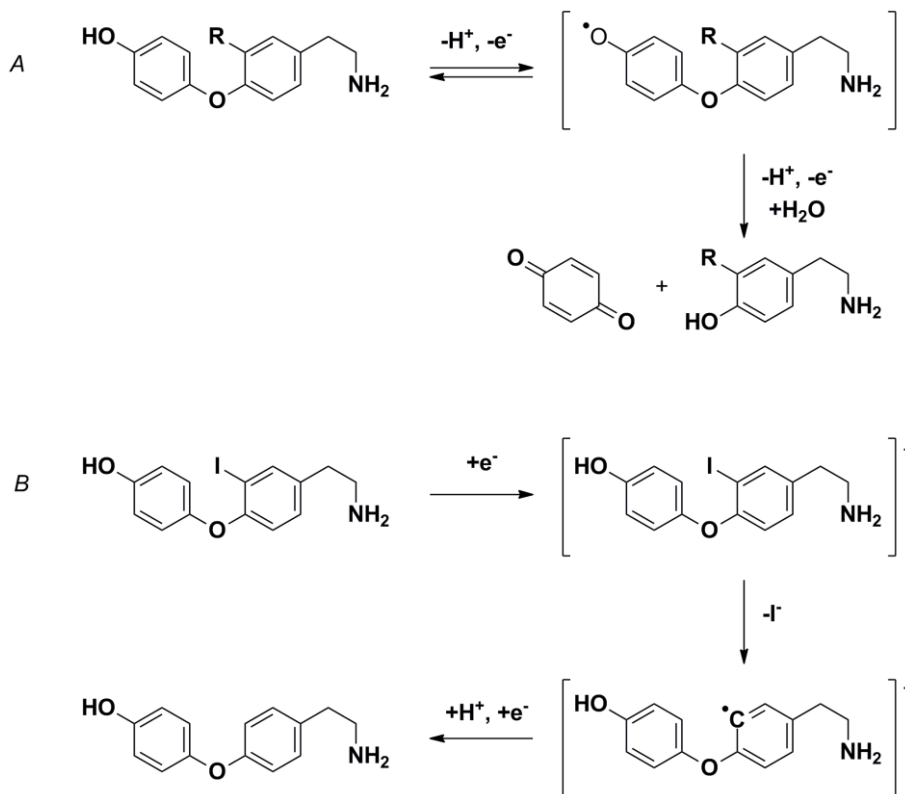
151 Figure 4 – pH studies, performed on universal buffer solution of a Britton-Robinson type, containing 0.12
 152 mM of T_1AM , with a GCE (the section above) and a HMDE (the section below). Similar results were
 153 obtained for T_0AM , 0.10 mM, for the case of the GCE (data not shown).

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155 The reductive process, for T₁AM, in a HMDE electrode, at pH 7, gives rise to a
 156 voltammetric signal with peak potential of ca. -1.2 V vs Ag|AgCl (Figure 3). A similar behavior to
 157 that obtained with the GCE was also noticed with the HMDE electrode (inlay of Figure 3), a slope
 158 of almost 1 in the logarithm plot of peak potential vs. scan rate ascribes to an adsorptive
 159 behavior.

160 Concerning the reductive reaction, the rate determining step should be a first electron
 161 transfer – an α value of 0.41 ± 0.05 , i.e. ca. 0.5, in the Tafel analysis agrees with such assumption
 162 – followed by the cleavage of the carbon-iodine bond releasing an iodide anion, and subsequent
 163 protonation of the carbon to which the iodine was bond (reaction B of Figure 5). Although in
 164 overall this would be a 2 electron 1 proton uptake, the first steps (the first electron transfer plus
 165 carbon-iodine cleavage) is rate determining which leads to the observed negligible pH
 166 dependence (Figure 4). However, when plotting peak potential vs. pH, there is a considerable
 167 slope above pH 8.2 (Figure 4), which might be explained as an extra removal of a proton from
 168 the reaction molecule. Considering this reductive mechanism for T₁AM where iodine plays part,
 169 one was not expecting to obtain a similar voltammetric signal for T₀AM. Such was the case, no
 170 signal was obtained in an effort to electrochemically reduce T₀AM in the HMDE.

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174 *Figure 5 – Reaction mechanisms. Reaction A – oxidative reaction on a GCE, Reaction B – reductive*

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reaction on a HMDE.

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177 These results not only show that it is possible to electroanalyze T₁AM and T₀AM but,
 178 furthermore, the analyses of T₁AM can be done with several different surfaces, since it can be
 179 performed either in a reductive or in an oxidative way. These results are proof-of-concept that
 180 may ultimately pave the way to the creation of low-cost reliable analytical methodologies for
 181 the quantitative analysis of T₁AM and/or T₀AM from biological and clinical samples, and

182 therefore provide the scientific and clinical community with better tools to understand the full
183 scope of their importance in human physiology.

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186 **Experimental section**

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188 All reagents used were of analytical grade and were used without further purification. pH studies
189 were performed with a universal buffer solution (of a Britton-Robinson type) composed of 0.1 mol L⁻¹
190 sodium phosphate, 0.1 mol L⁻¹ sodium acetate and 0.1 mol L⁻¹ sodium borate. The pH was adjusted to the
191 intended value with 6 mol L⁻¹ hydrochloric acid or 4 mol L⁻¹ sodium hydroxide. All aqueous solutions were
192 prepared using ultrapure water with resistivity not less than 18.2 MΩ cm at 298 K.

193 All voltammetric measurements were performed using a Metrohm 663 VA voltammetric stand
194 using a Ag|AgCl (KCl, 3 mol L⁻¹) reference electrode and platinum as the counter-electrode. Two working
195 electrodes were used: a HMDE (drop size ca. 0.52 mm²) and a GCE (area ca. 3.14 mm²).

196 The system was connected to a μAutolab II voltammetric system operated by the software GPES
197 v 9.4. All measurements were performed at room temperature. Solutions were deoxygenated with water-
198 saturated nitrogen for 10 min.

199 T₁AM and T₀AM were synthesized according to a previously published method.^[13]

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202 **References**

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